

Combined atomic force microscope and acoustic wave devices: application to electrodeposition.

J.-M. Friedt, L. Francis, K.-H. Choi, F. Frederix and A. Campitelli
friedtj@imec.be, campi@imec.be

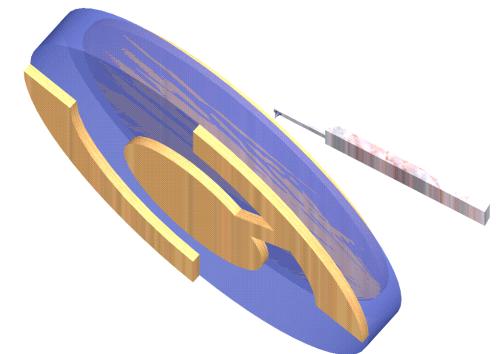
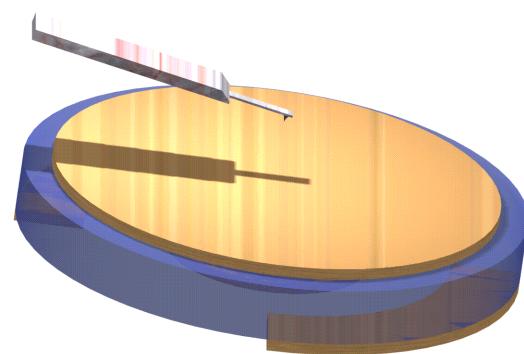
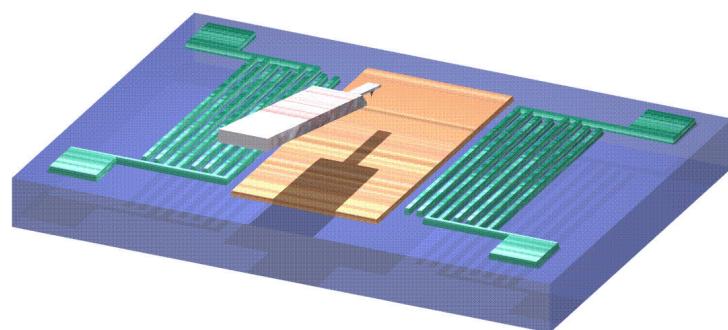
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Aim

Development of biosensors based on acoustic wave devices: requires to understand the sensing mechanism in liquid medium.

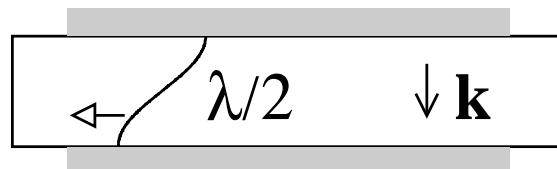
Biological reactions are too slow: use of electrodeposition (fast, reversible and more reproducible).

Look at the nm scale what is happening and relate the observations to the frequency variations.

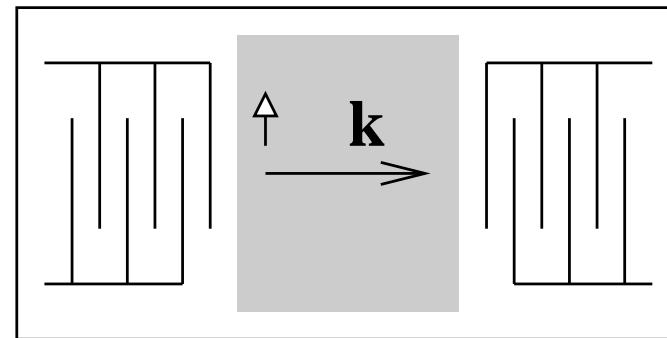


Principle

QCM ($c=\text{constant}$)



SAW device ($\lambda=\text{constant}$)

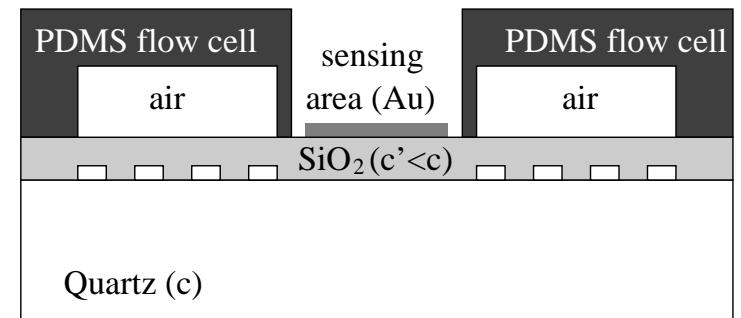


QCM: $\Delta m \rightarrow \Delta \lambda \rightarrow \Delta f$
SAW: $\Delta m \rightarrow \Delta c \rightarrow \Delta \Phi \rightarrow \Delta f$ } what about additional viscosity effects ?

Advantages of SAW:

- higher sensitivity (when properly designed)
- open back side for adding more sensing techniques
- sensing electrode is not used/polarized

Love mode device:

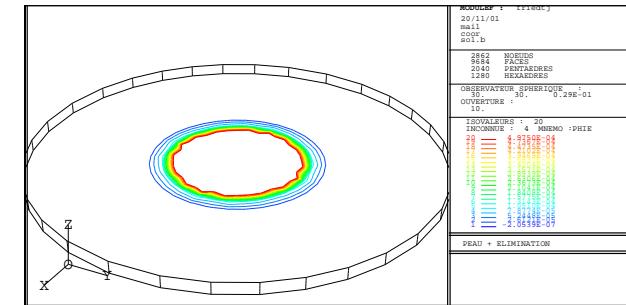


QCM/AFM combination

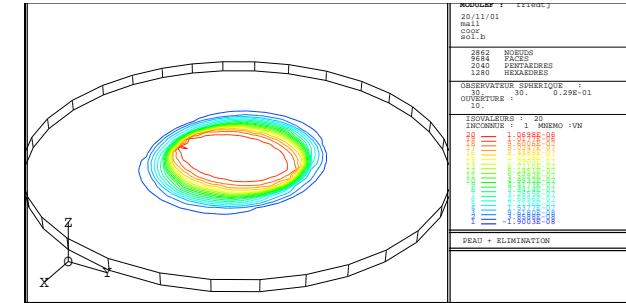
- static finite element analysis: out of plane displacement A is 0.1 pm
 - $A_{dynamic} = A_{static} \times Q \Rightarrow$ out of plane displacement is 0.3 nm ($Q \simeq 3000$)
 - in plane displacement is at most 3 nm, smaller than AFM pixel size
 - standing wave pattern between QCM and cantilever holder only disturbs the resonance frequency during approach
 - fundamental resonance frequency (5 MHz) is unstable and overtones of the QCM must be used

Use of commercial instruments:

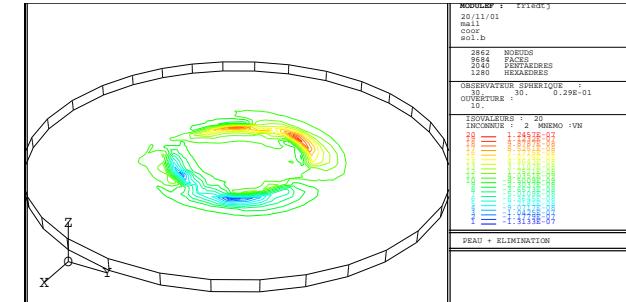
- Q-Sense (Göteborg, Sweden) for QCM-D monitoring (overtones 1, 3, 5, 7+Q factor)
 - Molecular Imaging (AZ, USA) AFM



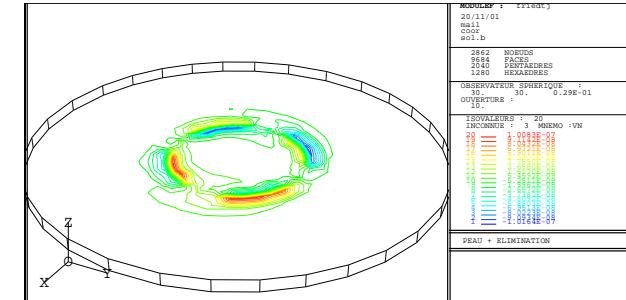
DC potential (0.5 V)



In-plane displacement (1 pm)

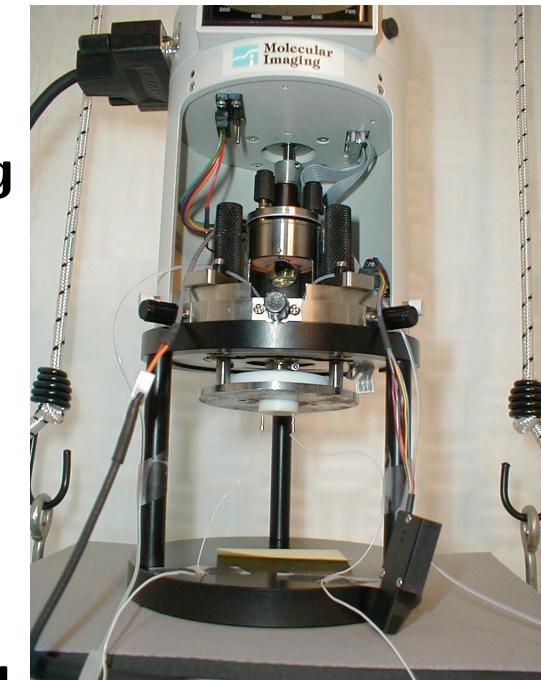
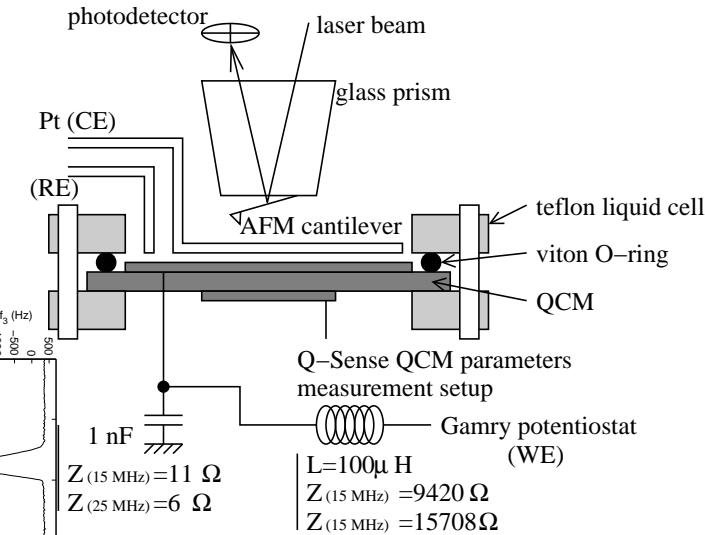
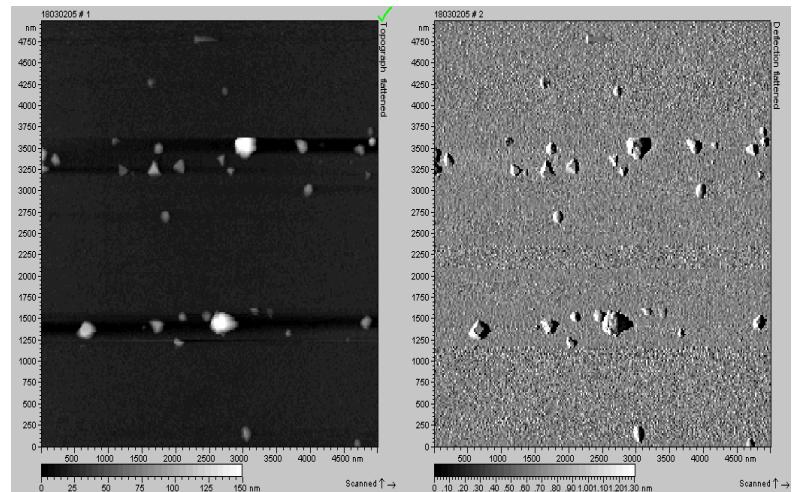
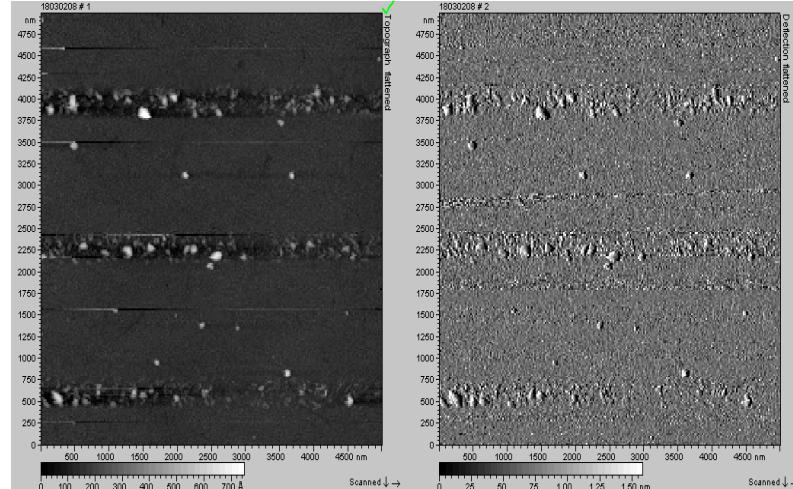


In-plane displacement (0.1 pm)



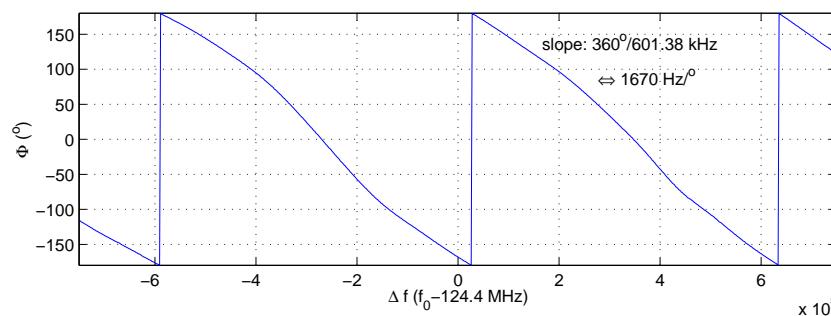
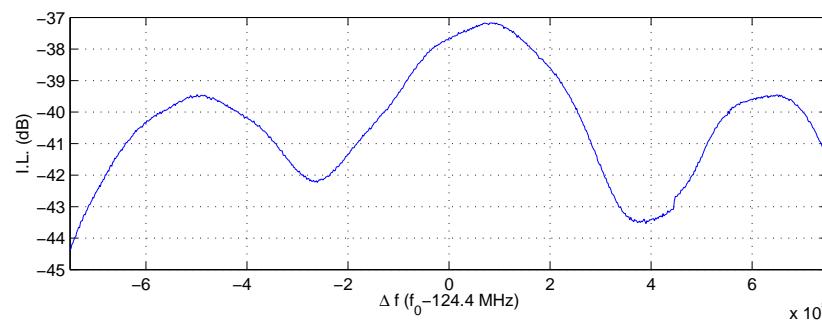
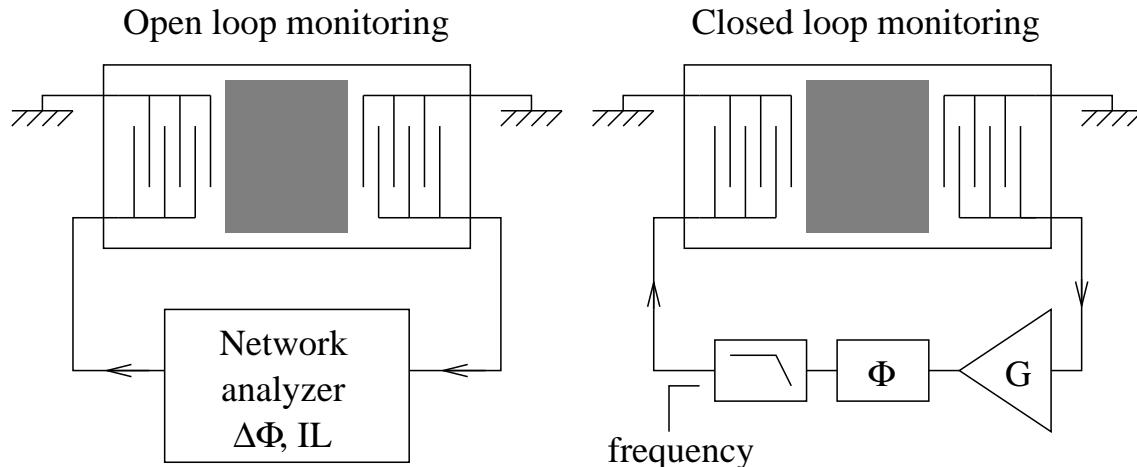
Out-of-plane displacements (0.1 pm)

Measurements



Rigid layer $\Rightarrow \Delta f_n/n \propto \Delta m_{layer}$ (low damping) with n : overtone number
 Viscous layer $\Rightarrow \Delta f_n/\sqrt{n} \propto \{\Delta m_{liquid}, \Delta m_{layer}\}$ (large damping)

Experimental setup

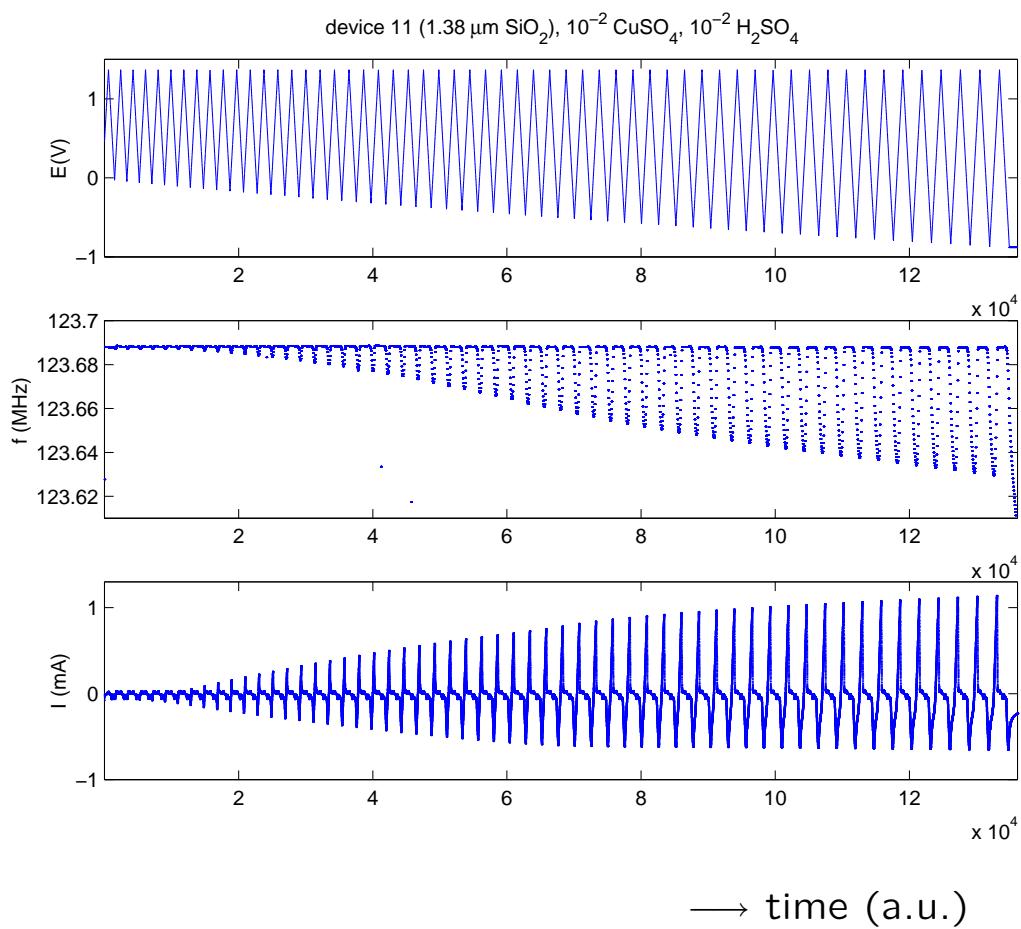


Open/closed loop operation:
requires a 4-port network
analyzer

PLL setup: compensate for
energy losses (and phase
shift)

Problem: liquid must *not*
reach the IDTs

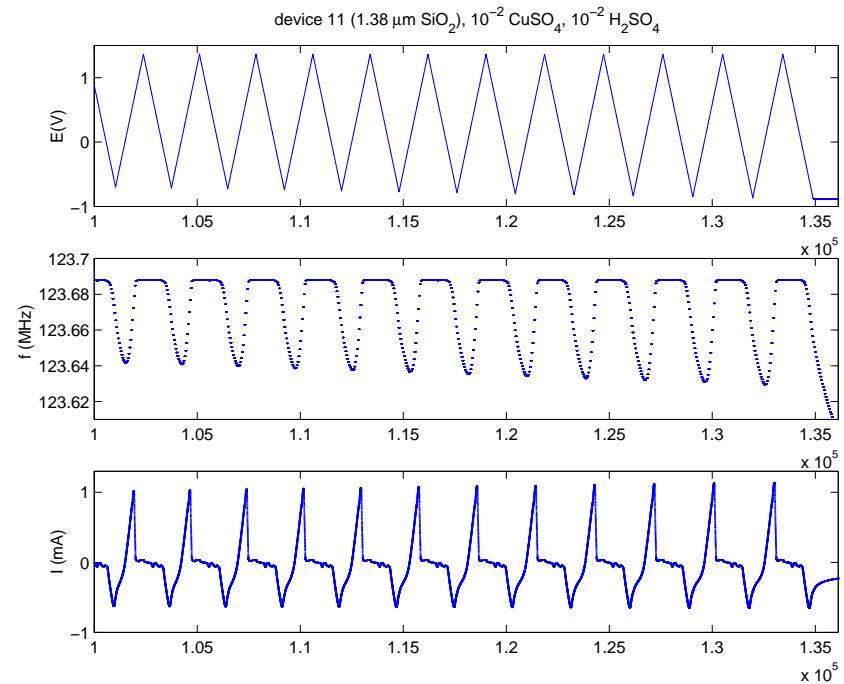
Measurements



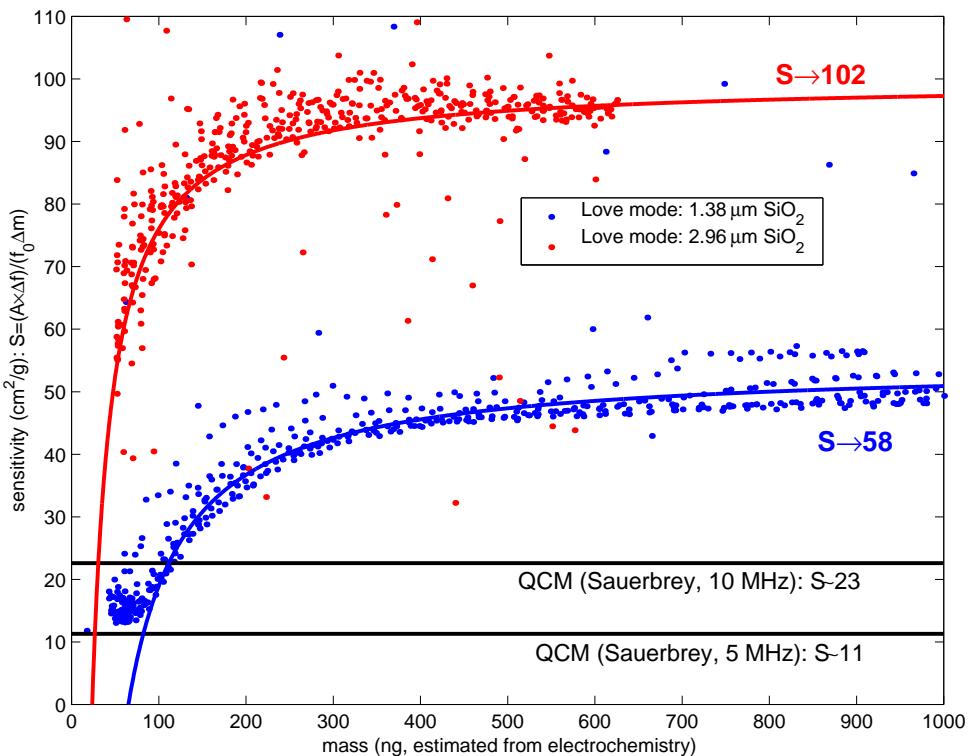
$$m_{Cu} = \frac{\sum I \times \delta t}{N \times e} \times \frac{M_{Cu}}{n_e}$$

$$N \times e = 96440 \text{ C: 1 Faraday}$$

$$M_{Cu} = 63.5 \text{ g/mol}, n_e = 2$$



Sensitivity estimates



$$S = \frac{\Delta f}{f_0} \times \frac{A}{\Delta m} \text{ cm}^2/\text{g}$$

A : sensing area ($3.2 \times 3.5 \text{ mm}^2$)

f_0 : center frequency (123.7 MHz)

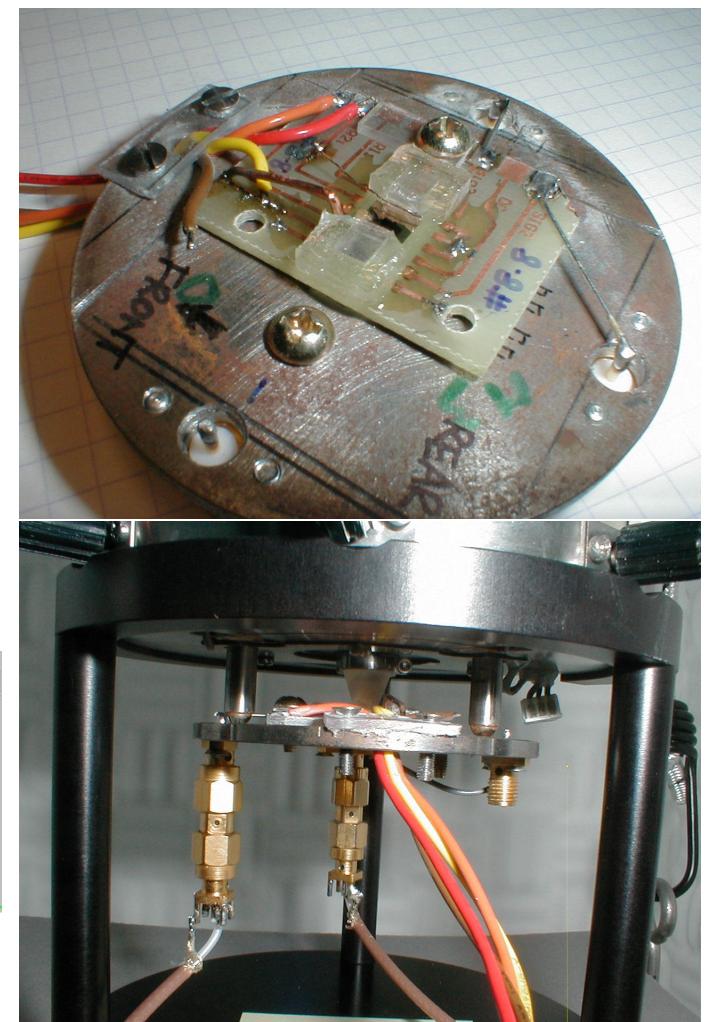
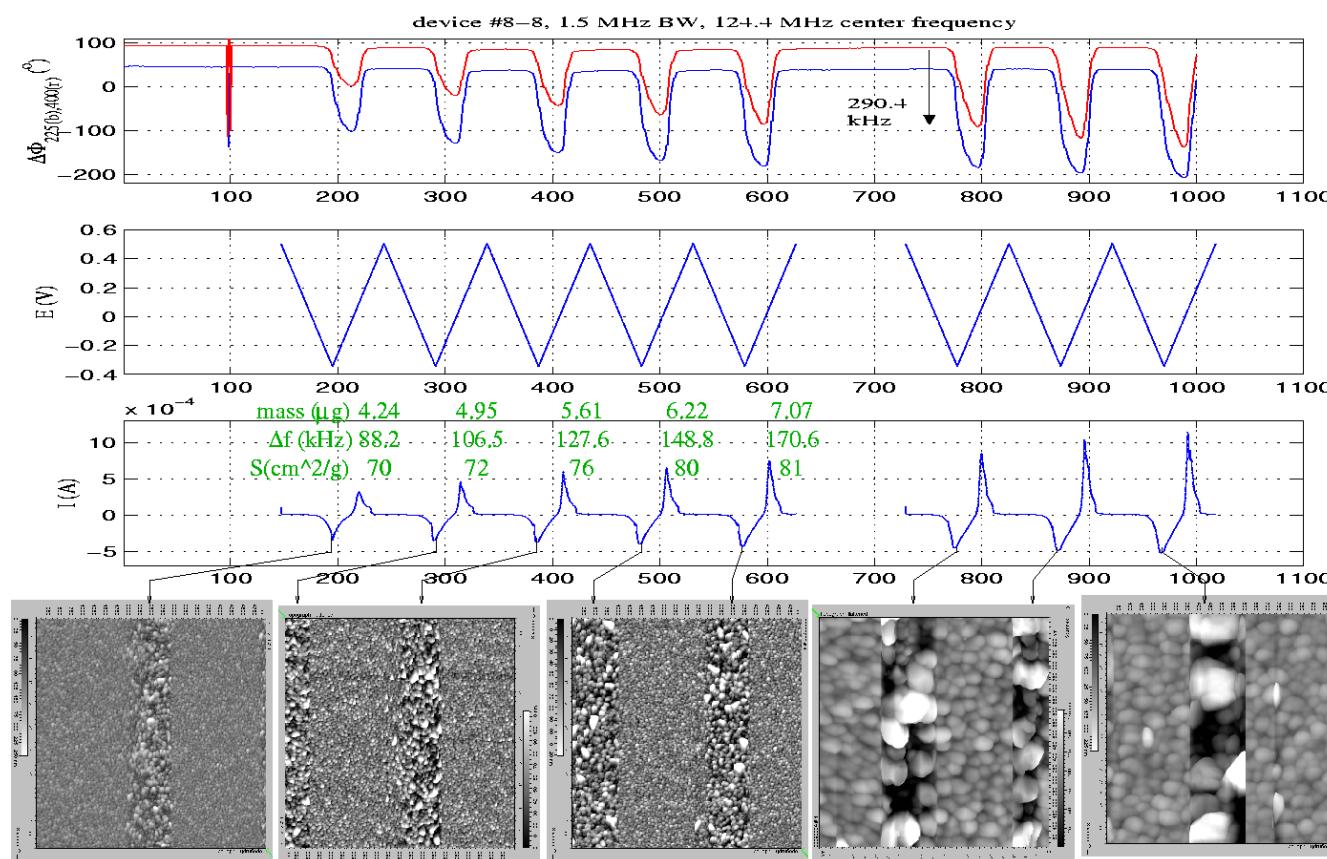
Δm : deposited mass (electrochemistry)

Δf : frequency variation

S assumed to be constant, $\forall \Delta m$. Good fit when including offset in the current measurement by the potentiostat \Rightarrow rigid mass.

AFM combination

Monitoring simultaneously $\Delta\Phi \Rightarrow \Delta f$, Δm and topography at the nm scale
 $\Rightarrow S \simeq 70..80$ for $\Delta m = 4.5..7.5 \mu\text{g}$ ($S_{QCM} \simeq 20 \text{ cm}^2/\text{g}$).



Conclusion and perspectives

- ability to independently measure deposited mass and frequency shift
 - estimation of the sensitivity: constant over the mass range analyzed
 - high sensitivity of Love mode device (~ 10 times more sensitive than QCM)
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- fluidics setup (IDTs protection)
 - application to biology: replace electrochemical cell by biochemical reactions
 - combination with other detection methods (SPR)